

# Mirror-Symmetric Tonotopic Maps in Human Primary Auditory Cortex

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## Summary

Understanding the functional organization of the human primary auditory cortex (PAC) is an essential step in elucidating the neural mechanisms underlying the perception of sound, including speech and music. Based on invasive research in animals, it is believed that neurons in human PAC that respond selectively with respect to the spectral content of a sound form one or more maps in which neighboring patches on the cortical surface respond to similar frequencies (tonotopic maps). The number and the cortical layout of such tonotopic maps in the human brain, however, remain unknown. Here we use silent, event-related functional magnetic resonance imaging at 7 Tesla and a cortex-based analysis of functional data to delineate with high spatial resolution the detailed topography of two tonotopic maps in two adjacent subdivisions of PAC. These maps share a low-frequency border, are mirror symmetric, and clearly resemble those of presumably homologous fields in the macaque monkey.

## Introduction

In the human brain, the term primary auditory cortex (PAC) refers to a region located in the transverse temporal gyrus or gyrus of Heschl (HG). Anatomically, PAC can be distinguished from the surrounding areas because of its granular (koniocortical) cytoarchitecture and its dense myelination (Hackett et al., 2001; Kaas and Hackett, 2000), features common to primary sensory areas in general. The exact number of subdivisions that form PAC remains unclear. Depending on histological criteria, what appears to correspond to the same auditory sensory cortex has been classified as one area (area 41, Brodmann, 1909) or further parcellated into two (areas

TC and TD: von Economo and Koskinas, 1925; areas KAm and Kalt: Galaburda and Sanides, 1980) or three (areas Te1.0, Te1.1, and Te1.2: Morosan et al., 2001) subdivisions. Even less is known on the functional differences between these presumed subdivisions.

In the macaque monkey, anatomical information of the cortical architecture could be complemented with functional information obtained using invasive electrophysiological recordings. Results from these studies support the hypothesis that two (AI, R) (Merzenich and Brugge, 1973; Morel et al., 1993) or three (AI, R, and RT) (Kaas and Hackett, 2000) subdivisions form a primary auditory cortical “core,” subserving a first stage of parallel processing of auditory information (Rauschecker et al., 1997). Neurons in these subdivisions respond best to tones at specific frequencies, exhibit narrow frequency response curves, and in at least two of these subdivisions (AI, R), form tonotopic maps. Analogously to retinotopic maps in the early areas of the visual cortex, these maps have a mirror symmetry. In AI, the most caudal of these fields, the tonotopic gradient from high to low frequencies is caudo-rostrally oriented. In R, located rostrally to AI, the tonotopic gradient is reversed such that AI and R share a low-frequency border that appears to coincide with the histologically defined border (Kaas and Hackett, 2000; Merzenich and Brugge, 1973; Morel et al., 1993). Similar to retinotopy in the visual system, tonotopy is not only a property of primary areas. Areas that belong to the so-called lateral “belt” and that subserve a second stage of the hierarchical sequence of auditory processing also display tonotopic organization, even though their neurons are less responsive to tones and prefer increasingly complex stimuli (Rauschecker et al., 1995, 1997).

A similar functional organization is expected in the human auditory cortex. Experimental evidence gathered in a number of functional neuroimaging investigations suggests a separation in “core” and “belt” areas (Di Salle et al., 2001; Seifritz et al., 2002; Wessinger et al., 2001) and the presence of multiple frequency-selective responses along the HG (Bilecen et al., 1998; Engelien et al., 2002; Lauter et al., 1985; Lockwood et al., 1999; Lütkenhöner and Steinsträter, 1998; Pantev et al., 1995; Romani et al., 1982; Schonwiesner et al., 2002; Talavage et al., 2000; Wessinger et al., 1997). However, all previous studies, including blood oxygenation level-dependent (BOLD) fMRI studies (Bilecen et al., 1998; Engelien et al., 2002; Schonwiesner et al., 2002; Talavage et al., 2000; Wessinger et al., 1997) at relatively high spatial resolution have so far failed to obtain detailed topographical representations of these frequency-selective responses. The failure to define spatial organization of frequency selective responses in the auditory cortex contrasts with the successes of fMRI in other sensory domains. In the visual domain, for example, fMRI studies have succeeded in defining the retinotopic layout and borders of early human visual areas (Sereni et al., 1995). By contrast, the number and the cortical layout of human tonotopic maps remain unknown.

In the present study, we combine ultra-high field MR

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imaging at high spatial resolution and improved specificity for functional mapping (Pfeuffer et al., 2002) with a cortex-based analysis of the functional images and depict the detailed layout of the tonotopic maps in the human PAC.

## Results

Subjects ( $n = 6$ ) were scanned with a 7 Tesla (T) MRI scanner. Auditory stimuli were 70 dB SPL tones at 0.5 and 3 KHz (subject #1), at 0.3, 0.5, 0.8, 1, 2, and 3 KHz (subjects #2, #4, #5, and #6), and 0.3, 1, 2, and 3 KHz (subject #3) and were binaurally presented according to an event-related stimulation scheme that minimizes interference of the scanner acoustic noise (Belin et al., 1999). Using single-shot echo-planar imaging (EPI), a linear surface coil, and an outer-volume suppression technique (Luo et al., 2001), we were able to “zoom in” on the subject’s left temporal lobe and acquire high-spatial resolution ( $1.2 \times 1.48 \times 2 \text{ mm}^3$ ) functional images of the auditory cortex. Functional images were coregistered to 3D anatomical volumes of the subject’s brain collected at 1.5T (see Magnetic Resonance Imaging).

For each subject, we computed a statistical map of the response of the auditory cortex to all the tones (see Data Analysis). The activation was mainly confined to the Heschl’s region, in a location that is in general agreement with what has been previously described as the location of the human primary auditory core (Brechmann et al., 2002; Di Salle et al., 2001; Engelien et al., 2002; Hall et al., 2002, 2003; Seifritz et al., 2002; Talavage et al., 2000; Wessinger et al., 2001). Because of the high spatial resolution and the suppression of the large vessel artifacts of 7T-fMRI, we found in the region delimited caudo-medially by the Heschl’s sulcus (HS) and rostro-laterally by the first transverse sulcus (FTS) the auditory activation to precisely follow the gray matter (Figure 1). Furthermore, its spatial layout showed a striking similarity to the layout of two cytoarchitecturally defined subdivisions of PAC (Te1.0 and Te1.1), as reported in recent anatomical studies (Morosan et al., 2001; Rademacher et al., 2001). Additional clusters with significant activation could be also observed outside this cortical core, especially in the adjacent caudal and lateral cortex (see Figures 1–5).

To investigate the cortical topography of frequency-selective BOLD-fMRI responses, we calculated best-frequency maps (see Data Analysis). In these maps, the color encodes the frequency of the tone that evoked the highest BOLD response (best-frequency). Maps were visualized on an inflated and a flattened representation of the subject’s cortex (Figures 2–5).

Figure 2 shows a cortical surface best-frequency map obtained by comparing the responses to tones at 0.5 and 3 KHz (subject #1). Clusters with highly selective BOLD responses to lower and higher frequency tones were observed in the Heschl’s region. In this subject, probably because of the presence of a duplicated HG, the most caudal aspect of the activation extended beyond the first (anterior) HG and occupied partially the second (posterior) HG. The spatial arrangement of the selective responses on the cortical surface suggested the existence of two mirror-symmetric representations

of the sound frequencies along a caudomedial-rostralateral direction. Assuming a smooth, continuous representation of the frequencies between 0.5 and 3 KHz, in the caudal region, the frequency selectivity gradient from high to low would be caudomedial-rostralaterally oriented; in the rostral region, the representation of the frequencies has a reverse order. The two maps’ relative anatomical location and the orientation of their tonotopic gradient suggest that these two regions might be the human homologs of monkey areas AI and R (hAI and hR) (Kaas and Hackett, 2000; Merzenich et al., 1973; Morel et al., 1993).

Figure 3A shows a best-frequency map obtained on the basis of the responses to six frequencies: 0.3, 0.5, 0.8, 1, 2, and 3 KHz (subject #2). In this case, the cortical topography of the tonotopic maps could be investigated in more detail, and the spatial arrangement of best-frequency clearly indicated the presence of two mirror-symmetric tonotopic maps. In a caudal region of the HG, proceeding from caudal to rostral locations, BOLD responses showed progressively reduced amplitude for high frequencies and increased amplitude for low frequencies. In a rostral region, BOLD responses exhibited an opposite pattern (Figure 3A). Additional clusters showing frequency-selective BOLD responses, but a less clear and less replicable topographical arrangement, could be observed lateral to these two regions (see also Figures 4 and 5). These clusters might belong to the so-called belt of auditory areas, in which responses to tones are weaker and less specific than in the primary areas (Rauschecker et al., 1995, 1997; Tian et al., 2001). Figures 3B and 3C illustrate a further analysis that we performed to investigate the frequency selectivity of auditory BOLD responses. Figure 3B shows the average best-frequency in a set of cortical clusters located in the two regions (a–f in Figure 3A). It can be seen that, moving along a line defined by connecting the spatial locations of clusters with highest selectivity, best-frequency monotonically decreases between “a” and “c” and monotonically increases between “c” and “f,” suggesting that the border between the two presumed tonotopic subdivisions is located approximately around “c.” Figure 3C displays frequency tuning curves of highly selective voxels from the same set of cortical clusters. Frequency tuning curves were obtained by calculating the amplitude of BOLD responses to tones at different frequencies (see Data Analysis) and indicate that the amplitude of BOLD responses monotonically decreases with increasing difference between stimulation frequency and best-frequency and further highlight the reversal of the tonotopic gradient around “c.”

To determine objectively whether the observed topographical arrangement of best-frequency reflects the existence of mirror-symmetric tonotopic maps, we adapted to our auditory data a field sign mapping method, as has been proposed for the analysis of retinotopic visual areas (Sereno et al., 1995) (see Data Analysis). Figure 4 shows the tonotopic-field sign maps we obtained in subject #2 (Figures 4A–4C) and subject #3 (Figure 4D). Blue color in the caudal area (hAI) indicates that the direction of the local low-to-high tonotopic gradient follows the direction indicated by the arrow (see insert in Figure 4A). Conversely, green color in the rostral area (hR) indicates a mirror representation of the low-

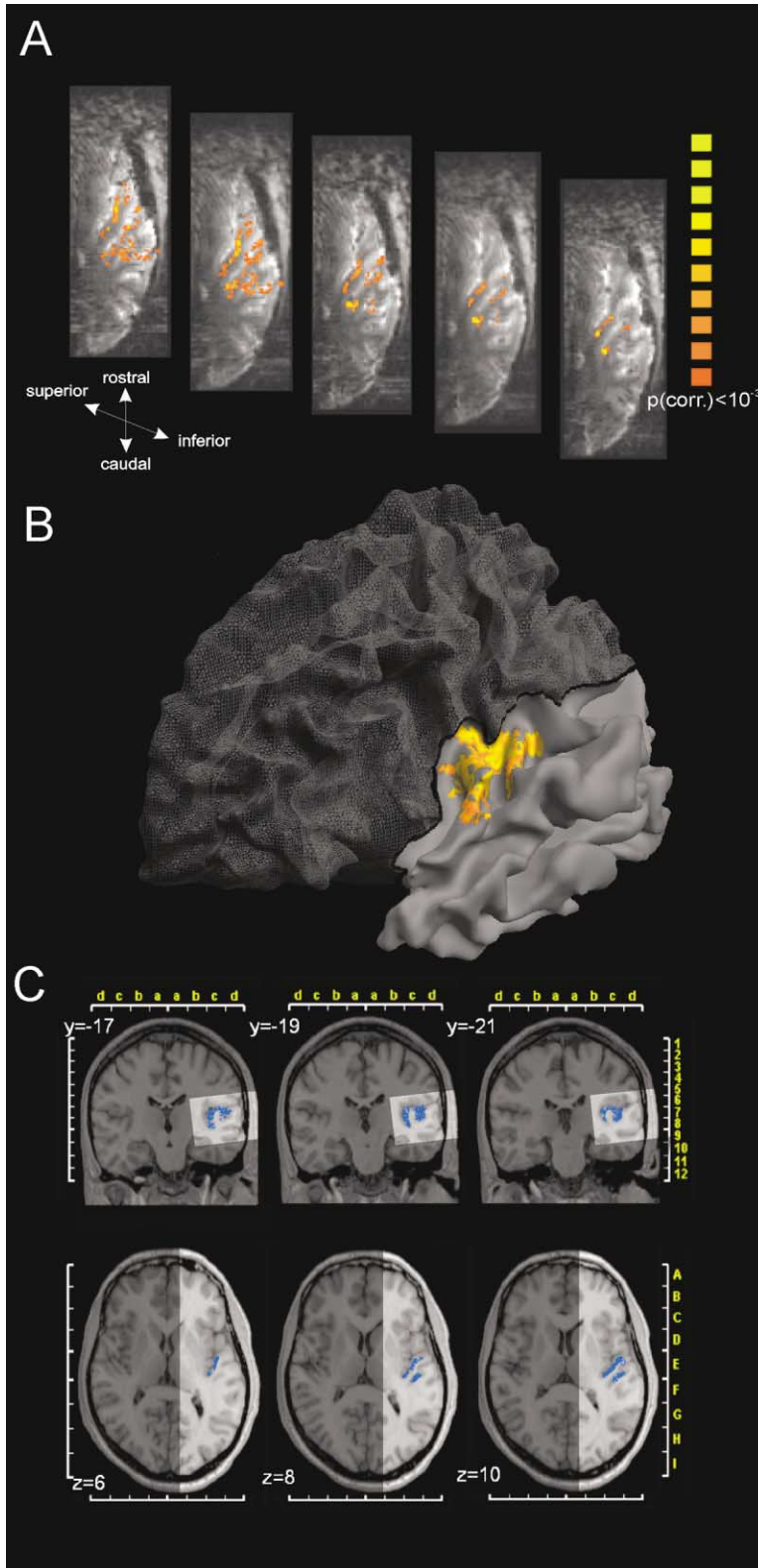


Figure 1. Localization of the Primary Auditory Cortex at 7 Tesla

A statistical map of the overall auditory cortex response to six frequencies (subject #2, frequency range 0.3–3 KHz) is superimposed on selected transverse echo-planar-imaging slices collected at 7T (A), on a mesh reconstruction of the subject's cortex, after part of the parietal lobe has been virtually removed for a better visualization of the activation in the Heschl's gyrus (B) and on coronal ( $y = -17, y = -19, y = -21$ ) and transverse ( $z = 6, z = 8, z = 10$ ) anatomical slices in standard Talairach space (C). In (C), lighter gray indicates the region of temporal lobe that was covered by the functional slices.

to-high local tonotopic gradient. These results confirmed our previous observations, showed a high reproducibility both for intrasubject (Figures 4B and 4C) and intersubject (Figures 4A and 4D, see also Figure 5) com-

parisons, and allowed us to outline the low-frequency border shared by the two areas (see dotted lines in Figure 4) in correspondence of the reversal of the field sign (Sereni et al., 1995).

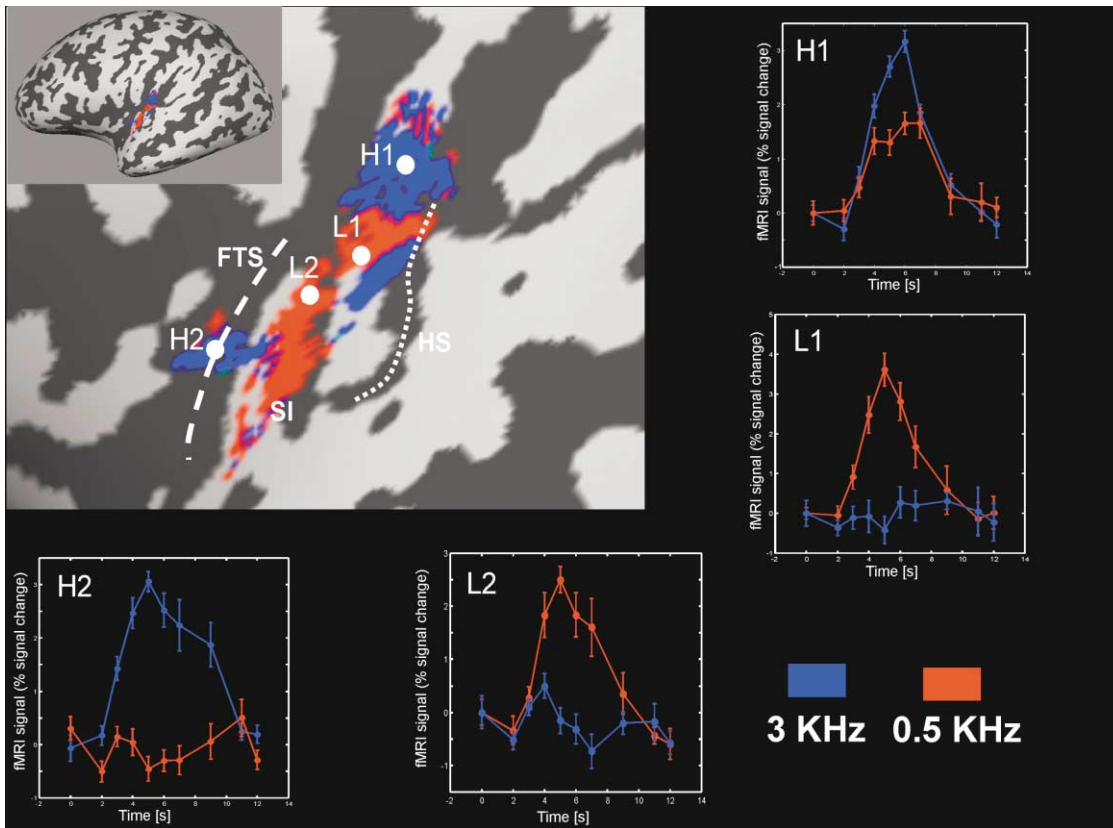


Figure 2. Spatial Layout and Average Time Courses of Frequency-Selective Responses in the Primary Auditory Cortex

A best-frequency map (subject #1; statistical analysis based on two frequencies [3 KHz, blue; 0.5 KHz, red]) is displayed on an inflated representation of the subject's cortex. In a caudal region of the activated auditory cortex, cortical clusters responding preferably to 3 KHz tones are located caudo-medially (H1), and cortical clusters responding preferably to 0.5 KHz tones are located rostro-laterally (L1). In a rostral region, cortical clusters responding preferably to 3 KHz tones are located rostro-laterally (H2), and cortical clusters responding preferably to 0.5 KHz tones caudo-medially (L2). Error bars indicate standard error of the mean. Note that this spatial arrangement of frequency-selective responses is compatible with the existence of two mirror-symmetric tonotopic maps with a rostro-caudal axis. FTS = first transverse sulcus; HS = Heschl's sulcus; SI = sulcus intermedius.

Figures 5 illustrates the cortical best-frequency maps and corresponding PAC subdivisions (in standard anatomical projections, Talairach and Tournoux, 1988) in subjects #4, #5, and #6. Maps and PAC subdivisions were obtained using identical methods and an identical set of six frequencies as in subject #2 (Figure 3) and provide a further confirmation of the reproducibility of our results. It can be noticed that, although the activation often occupies a larger expanse of cortex, two mirror-symmetric gradients (high-to-low, low-to-high) of best-frequencies can be consistently observed moving from the caudomedial extremities of the HS to rostrolateral locations along the first transverse sulcus FTS.

## Discussion

Our ultra-high magnetic field imaging study provides new, compelling evidence for functional subparcellation of human PAC and thus extends previous results obtained invasively in monkeys to the human brain. Two mirror-symmetric representations of sound frequency appear to be contained in a region that significantly responds to simple tones and that is presumably in-

cluded within the cytoarchitectonically delineated primary auditory sensory cortex.

Several reasons might explain why these maps could be convincingly observed in our, but not in previous, BOLD-fMRI studies. First, the silent event-related paradigm allowed us to image the auditory cortex without the interference of the loud (~100 dB) background acoustic noise, which might have been a severe limitation in previous studies using a conventional blocked or a continuous stimulation paradigm (Bilecen et al., 1998; Schonwiesner et al., 2002; Talavage et al., 2000; Wessinger et al., 1997). Second, we examined the spatial pattern of BOLD responses to up to six different frequencies using a cortical-surface-based reference system. In previous studies (Bilecen et al., 1998; Engelien et al., 2002; Talavage et al., 2000; Wessinger et al., 1997), inferences on the cortical layout of one or multiple tonotopic maps have been based only on the analysis of the relative displacement of the foci of BOLD responses to a very small number (two or three) of frequencies or ranges of frequencies. In addition, analysis in all previous studies has been conducted only on sets of two-dimensional (2D) slices or in a three-dimensional (3D) brain volume

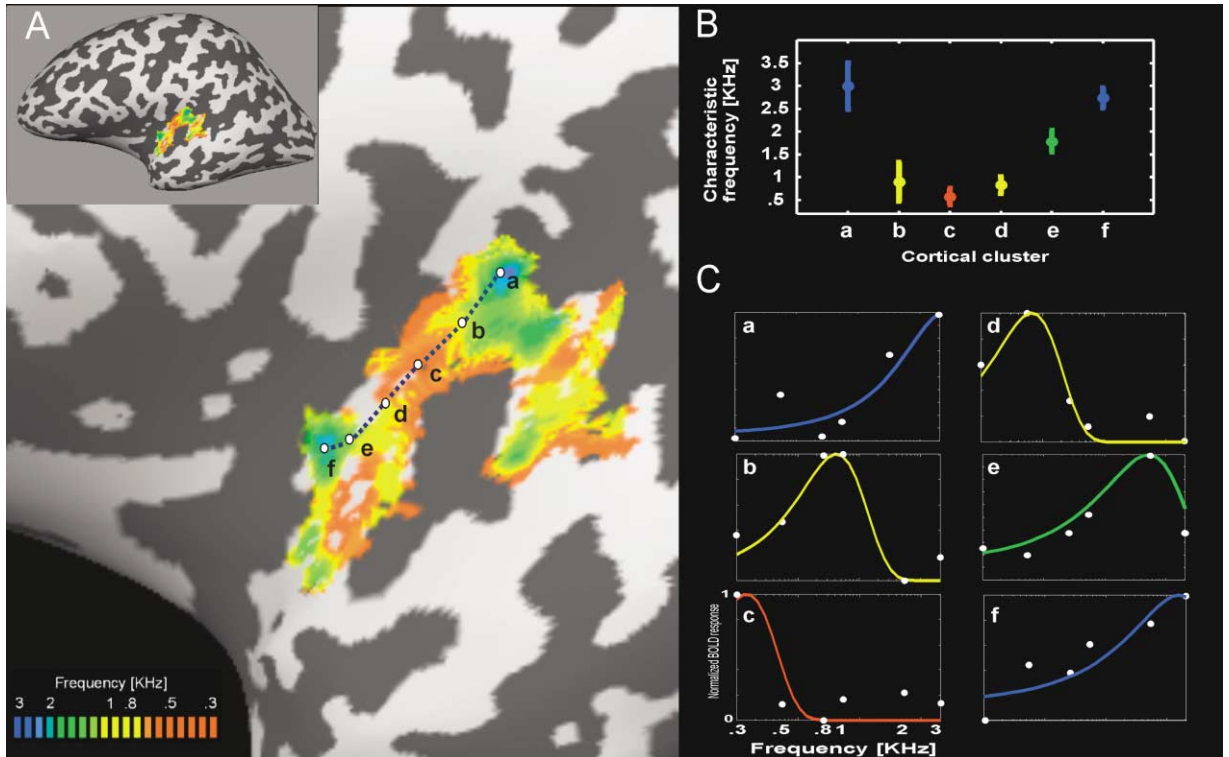


Figure 3. Spatial Layout, Best-Frequency, and Tuning Curves of Frequency-Selective Responses in Primary Auditory Cortex

(A) A best-frequency map (subject #2; statistical analysis based on six frequencies [0.3, 0.5, 0.8, 1, 2, and 3 KHz]) is displayed on an inflated representation of the subject's cortex. Color indicates the stimulus frequency that evoked the highest BOLD response. The spatial arrangement of best-frequencies reveals the existence in the human primary auditory cortex of two continuous representations of frequency (tonotopic maps) presenting a mirror symmetry along the rostral-caudal direction.

(B) Average best-frequency in a set of  $\sim 5$  mm<sup>2</sup> cortical clusters (a, b, c, d, e, and f) located in the activated PAC. Error bars indicate the standard deviation computed over best-frequencies of individual voxels indexed by these cortical clusters. In the caudomedial region (clusters a–c), the best-frequency gradient from high to low is caudo-rostrally oriented. In the most rostral region (clusters c–f) the best-frequency gradient reverses. The two tonotopic maps appear to share a common low-frequency border approximately in “c” (see also Figure 4).

(C) Frequency tuning curves for highly selective voxels from the clusters a, b, c, d, e, and f. Continuous lines show the fitting of the normalized amplitude of event-related averages of the BOLD responses to the six frequencies with a Gaussian function (see Data analysis).

and was not based on an explicit representation of the subject's cortex as in the present study. Finally, because of the lower contrast-to-noise and lower inherent image signal-to-noise, the spatial resolution utilized in the previous studies conducted with conventional low-field fMRI was significantly coarser compared to our 7 Tesla investigation. More importantly, spatial accuracy (specificity) of BOLD mapping signals achievable with conventional low-field fMRI is expected to be significantly degraded at lower magnetic field relative to 7T (Ugurbil et al., 2003) and might have been insufficient for an adequate mapping of the small auditory areas.

Our findings are consistent with those of studies in which intracortical auditory event-related potentials (ERPs) were recorded using depth electrodes (Liegeois-Chauvel et al., 1991, 1994). In Liegeois-Chauvel et al. (1994), the PAC was partitioned into two subdivisions, labeled respectively as the “extreme dorso-posterior-medial” region (located in the extreme posterior tip of the Heschl's gyrus) and the “dorso-posterior intermediate” region (located few millimeters more anterior and more lateral to the other region). The anatomical locations of these subdivisions and their relative displacement closely resemble those of our noninvasively mapped

caudal and rostral subdivisions of PAC. The orderly frequency progression in the HG reported in another study using implanted microelectrodes in surgical patients (Howard et al., 1996) is also compatible with the tonotopic gradient in our caudal subdivision.

Electroencephalography (EEG) and magnetoencephalography (MEG) also contributed to the investigation of tonotopy of the human auditory cortex (Huottilanen et al., 1995; Lütkenhöner and Steinsträter, 1998; Lütkenhöner et al., 2003a; Pantev et al., 1995, 1996; Romani et al., 1982; Scherg et al., 1989; Yamamoto et al., 1992). Typically, in these studies, the tonotopic layout of an auditory cortical field is inferred by relating changes in sound frequency to shifts of orientation or spatial locations of dipoles, which are assumed to generate the scalp distribution of the evoked potential or magnetic field in specified time windows. Several difficulties arise when trying to link these frequency-dependent dipole shifts with the pattern of hemodynamic activation observed in our fMRI study. First, fMRI and EEG/MEG are based on very different biophysical mechanisms and may reflect different aspects of neuronal activity (Dale and Halgren, 2001). Second, because the neural activities of at least two closely located fields of the PAC are

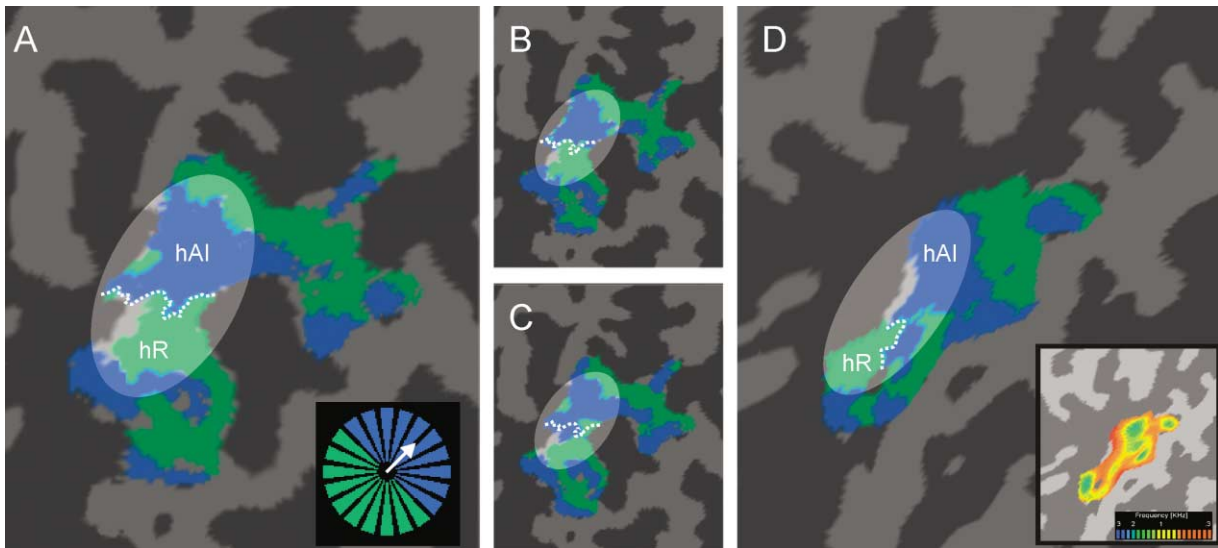


Figure 4. Tonotopic Field Sign Maps of the Human Primary Auditory Cortex

Blue and green colors indicate maps with mirror-symmetric representation of the low-to-high tonotopic gradient (see Data Analysis for details). The reversal of the field sign defines the low-frequency border between area hAI and area hR (see dotted line). In (A)–(C) tonotopic field sign maps of subject #2 were obtained from the best-frequency map shown in Figure 3 (A) and from best-frequency maps computed using only the first (B) or the second (C) half of collected data, respectively. The insert in (D) shows the best-frequency map used to compute the field sign map of subject #3.

likely to present a consistent temporal overlap (Liegeois-Chauvel et al., 1994), their modeling with equivalent dipoles may be problematic (scalp-recorded fields produced by multiple, closely located, simultaneously active current sources and those produced by a single dipole cannot be easily distinguished). Third, because tonotopic cortex in the different auditory subdivisions is variously oriented, the observed shift of dipole locations may result from a complexly weighted contribution of their activity rather than being univocally related to the activity of a single subdivision (Eggermont and Ponton, 2002). Finally, many of the EEG/MEG studies on tonotopy have focused on a component, the N100(m), which is likely to represent activity of secondary auditory areas (planum temporale) and whose frequency dependence is still controversial (for a recent discussion of the conflicting results on the tonotopy of the N100, see Lütkenhöner et al., 2003a).

Notwithstanding these cautionary remarks, it is interesting to note that the dipole-based source localization of the scalp-recorded auditory evoked potential and magnetic field recorded about 19–30 ms after stimulus onset (Scherg et al., 1989; Schneider et al., 2002; Pantev et al., 1995; Yvert et al., 2001) is compatible with our fMRI-based localization of the PAC. Opposite frequency-dependent shifts of the equivalent dipole location, however, have been reported which are either compatible with the tonotopic gradient of hAI (N19m-P30m response in Scherg et al., 1989) or with the tonotopic gradient of hR (Pam response in Pantev et al., 1995). This might be explained by methodological differences but also by assuming that (1) in the human PAC two closely located primary cortical fields are present, (2) their tonotopic gradient is oriented in opposite directions, and (3) their activity overlaps in time. The first two

points are supported by our data; the third is supported by intracortical recordings (Liegeois-Chauvel et al., 1994) and by recent analyses of transient (Lütkenhöner et al., 2003b) and steady-state MEG responses (Gutschalk et al., 1999). Future studies combining high spatial resolution fMRI and EEG-MEG in the same subjects may help in relating results on tonotopy obtained using a single neuroimaging technique.

The tonotopic maps of the human PAC as revealed by our BOLD fMRI measurements are remarkably similar to the tonotopic maps as described in invasive electrophysiological studies in the macaque monkey (Kaas and Hackett, 2000; Merzenich and Brugge, 1973; Morel et al., 1993). Maps of neural best-frequencies in these as well as in studies in other animal species are typically obtained at low sound levels, 0–20 dB above the response threshold. In contrast, our maps were obtained at a sound level of 70 dB SPL. Whereas this intensity level is lower than levels used in previous fMRI investigations of tonotopy, it is still considerably higher than the intensity of stimuli typically used in electrophysiological recordings in animals.

It is known that frequency selectivity decreases with increasing sound level, suggesting that weaker stimuli are better suited to reveal tonotopy. However, fMRI, in comparison to single-cell recording, is less sensitive to weak and spatially restricted activity. Stronger stimuli are, thus, required to elicit measurable responses. On the other hand fMRI provides extended (though discrete) coverage of large volumes. Therefore data describing an extended region can be statistically integrated across space to reveal tonotopic organization. The optimal sound level for mapping tonotopy with fMRI is, thus, expected to be higher than for single-cell recording.

It should be noted, however, that several investiga-

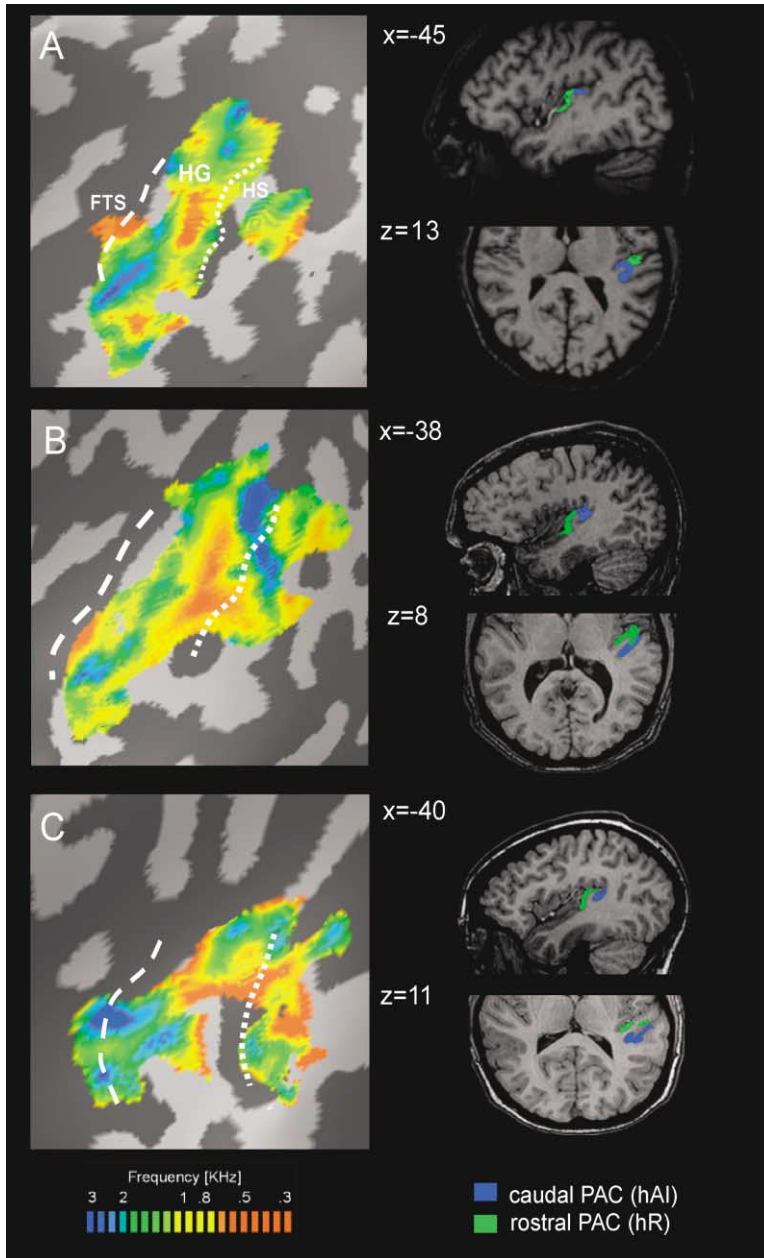


Figure 5. Best-Frequency Maps and Corresponding PAC Subdivisions in Subjects #4, #5, and #6

([A–C], left column) Cortical best-frequency maps are displayed on an inflated representation of the subjects' cortex (subject #4 [A], subject #5 [B], subject #6 [C]). Statistical analysis is based on six frequencies (0.3, 0.5, 0.8, 1, 2, and 3 KHz), and color indicates the stimulus frequency that evoked the highest BOLD response. ([A–C], right column) PAC subdivisions, as defined by the mirror-symmetric tonotopic maps, are visualized on selected sagittal and transverse anatomical slices in standard Talairach space. FTS = first transverse sulcus; HG = Heschl's gyrus; HS = Heschl's sulcus.

tions in anesthetized animals have shown that stimuli at high intensity levels evoke reduced response rates in a percentage of neurons in the primary auditory cortical field (cat: Schreiner et al., 1992; Heil et al., 1994; Phillips et al., 1994; ferret: Kowalski et al. 1995). Furthermore, in the anesthetized cat, a tonotopic layout is observed with near-threshold stimuli but may be absent or altered at high intensity levels (Phillips et al., 1994).

Our findings demonstrate for awake humans that responses are still selective to frequency and that tonotopic maps exist in human PAC at 70 dB SPL. These findings are compatible with the results of a recent investigation of frequency and intensity response properties of single neurons in the auditory cortex of the behaving macaque monkey (Recanzone et al., 2000). Frequency response areas of AI neurons reported in this

study indicate for intensity levels around 70 dB SPL that neurons respond to a relatively broad range of frequencies. However, their response is still highest at frequencies close to the frequency that produces a driven response at the lowest intensity (Recanzone et al., 2000). Our approach of computing the best-frequency maps based on the frequency evoking the highest BOLD response is robust to a partial loss of frequency selectivity and to a certain degree of overlap of responses, which is expected at the intensity level of our stimulus. Further investigations employing a broader combination of intensities and frequencies in human experiments will help test this possibility.

More generally, it should be noted that BOLD fMRI measurements reflect the hemodynamic changes related to the spiking and subthreshold activity of large

ensembles of neurons (Logothetis et al., 2001) and that, even at the relatively high spatial resolution achievable at ultra-high magnetic field, the spatial scale of the investigation is much coarser than in invasive electrophysiological recordings. Caution should thus be taken in judging similarities and dissimilarities between fMRI results and results from electrophysiological investigations typically based on spike counts of single units.

Importantly, our results are consistent with recent studies of the auditory cortex in anesthetized animals that employed optical imaging, a technique based on physiological principles closely related to BOLD fMRI (Harel et al., 2000; Versnel et al., 2002). In Harel et al. (2000), tonotopic maps of the auditory fields of the chinchilla that resembled those derived electrophysiologically (Harrison et al., 1996) were obtained using stimuli identical to ours and sound levels up to 80 dB SPL. In Versnel et al. (2002) optical tonotopic maps of the ferret's auditory cortex were shown to be largely independent of the (suprathreshold) sound level and also of the type of narrowband stimulus used (pulsed, amplitude-, or frequency-modulated) and the modulation rate. Compared to these maps, the tonotopic layout of our human tonotopic maps appears to show a greater intersubject variability. This is possibly a consequence of the greater anatomical variability of the human auditory cortex but also of the fact that our subjects were awake and that response properties of neurons are more variable or subject to modulation in the awake state than in the anesthetized state. Future studies employing a wide range of techniques in the same animal will be particularly relevant in elucidating the relation between electrophysiologically derived and hemodynamic/metabolic tonotopic maps and their dependence on the state of the animal.

Our findings have a great practical relevance for future studies of human audition. The identification of primary auditory subdivisions represents an essential step in understanding the cortical organization of the human brain underlying the perception of sound, including speech and music. Because of the great interindividual anatomical variability of the Heschl's region (Penhune et al., 1996) and because of the weak correspondence between commonly used anatomical landmarks and architectonically defined subdivisions (Morosan et al., 2001), this identification can only be obtained with functional mapping in individual brains. In few pathological cases this might be carried out invasively using intrasurgical event-related potential recordings (Liegeois-Chauvel et al., 1991, 1994). Our results demonstrate that with silent event-related fMRI at high spatial resolution and tonotopic mapping, such information can be unambiguously obtained in normal volunteers.

The specific neurocomputational role of these two representations of sound frequency within PAC cannot be explained exclusively on the basis of available data. Various invasive methods demonstrated the existence of tonotopic maps of PAC in a number of species (Harel et al., 2000; Kaas and Hackett, 2000; Merzenich and Brugge, 1973; Merzenich et al., 1973; Morel et al., 1993; Recanzone et al., 1999) and their functional role in extracting spectral features of a sound (Read et al., 2002; Scheich, 1991). In humans, as in primates (Kaas and Hackett, 2000), it is likely that the two frequency maps

subserve a first stage of parallel processing of auditory information and initiate downstream processing in the auditory "what" (rostral) and "where" (caudal) parallel functional streams (Rauschecker and Tian, 2000; Romanski et al., 1999).

We expect that tonotopic mapping in combination with a large variety of auditory stimuli will help clarify the exact contribution of these two subdivisions to auditory processing and, more generally, how topographically encoded information on sound frequency is combined with different and variously encoded information on other features of the auditory stimuli, such as duration, amplitude, bandwidth, and modulation (Brechmann et al., 2002; Di Salle et al., 2001; Hall et al., 2002; Seifritz et al., 2002; Wessinger et al., 2001) and with mechanisms of sound localization (Alain et al., 2001; Warren et al., 2002).

## Experimental Procedures

### Subjects

Six adult subjects (four male, two female, ages 23–38) gave their informed consent and participated in the study. Subjects were all right handed and had normal audition.

### Magnetic Resonance Imaging

Functional imaging was performed at the Center for Magnetic Resonance Research (Minneapolis, MN) in a 90 cm bore 7 Tesla magnet (Magnex Scientific, Abingdon, UK) operated with a Varian (Palo Alto, CA) console. A linear surface coil (12 cm diameter) and a single-shot Gradient Recalled Blipped Echo Planar Imaging (EPI) sequence (echo time (TE) = 27 ms, flip angle (FA) = 90°, TR = 20 s) were used for collecting high-resolution functional images of the left temporal lobe. Localized adjustments of the first order shims, and when needed of the second order shims, were performed in the temporal cortex with FAST(EST)MAP (Gruetter and Tkac, 2000). In order to acquire single-shot high-resolution EPI images, an outer-volume suppression technique with adiabatic pulses (see Luo et al., 2001; Pfeuffer et al., 2002, for details) was used, yielding a reduced field-of-view of 15.36 cm (antero-posterior) × 6.50 cm (left-right) and a nominal resolution of 1.20 × 1.48 × 2.00 mm<sup>3</sup>.

Within each 7T functional session, T1-weighted EPI images (obtained with an inversion preparation module, inversion time TI = 1.5 s, FA = 90°, TE = 27 ms) were also collected at the same slice locations. These images were used to coregister 7T data sets with a whole-head 3D anatomical dataset obtained from the same subjects using a conventional 1.5T clinical scanner (MAGNETOM Vision; Siemens, Erlangen, Germany) and a three-dimensional T1-fast-low-angle shot (FLASH) sequence (180 slices, TR = 30 ms; TE = 5 ms; FA = 40°; FOV = 256 × 256 mm<sup>2</sup>; matrix = 256 × 256; voxel size = 1 × 1 × 1 mm<sup>3</sup>). After coregistration, the 1.5T 3D data set was used for visualization of the functional 7T data (see Data Analysis).

### fMRI and Stimulation Paradigm

Auditory stimuli consisted of binaural 3 s sine tones with the carrier frequency at 0.3, 0.5, 0.8, 1, 2, or 3 KHz, pulsed with a 8 Hz square wave (rise/fall time = 5 ms, plateau = 30 ms, interstimulus interval [ISI] = 50 ms). Stimuli were generated and delivered using a system that included a personal computer, custom-made software, a commercial sound card, and a commercial MR-compatible stimulation device (Commander XG, Resonance Technology Inc.), which uses an air-conducting tube in combination with a nonmagnetic piezoelectric transducer. Before the measuring sessions, the stimulation system was calibrated by means of a condenser microphone (Larson Davis, 2540), a precision sound level meter (Bruel & Kjaer, 2231), and a calibrator (Larson Davis, CA250). The system does not induce artifacts in MR images, has a flat frequency response, and accurately preserves tone frequencies in the range of the stimulation frequencies used (0.3–3 KHz). The intensity of the output stimulus was set to 70 dB SPL for all subjects and for all the frequencies. Special



padded headphones provided an overall attenuation of  $\sim 30$  dB to the environmental noise.

Functional images were collected using a stroboscopic event-related scheme that has been shown to avoid any interference of the scanner acoustic noise (Belin et al., 1999). During a scanning session several functional runs were collected. In each separate run, a tone at one of the six frequencies was used for stimulation. Subjects underwent two (with tones at 0.5 and 3 KHz, subject #1), six (with tones at 3, 0.3, 1, 2, 0.8, and 0.5 KHz, subjects #2, #4, #5, and #6) or four (with tones at 0.3, 3, 2, and 1 KHz, subject #3) functional runs. A functional run included 48 multislices (20 slices, matrix size =  $128 \times 44$ , total acquisition time = 1.35 s) EPI measurements. Each EPI measurement was collected at regular 20s intervals with an auditory stimulus being presented at variable offsets (0, 2, 3, 4, 5, 6, 7, and 9 s) before each scan. This acquisition scheme allowed the reconstruction of the entire time course of six stimulus-evoked BOLD responses for each run/frequency.

#### Data Analysis

Functional and anatomical images were analyzed using Brain Voyager 2000 (Brain Innovation, Maastricht, The Netherlands). After preprocessing (interscan slice time-correction, 3D motion correction, high-pass filtering), functional time series were interpolated to  $1 \times 1 \times 1$  mm<sup>3</sup> and coregistered to 3D anatomical images that were used for automatic cortical surface reconstruction, inflation, and flattening and for the generation of cortical masks that were used as a constraint for the analysis of functional time series (Kriegeskorte and Goebel, 2001; Formisano et al. 2002). Statistical maps were obtained on the basis of a single-subject analysis. For each subject, a general linear model (GLM) that included a linear predictor for each frequency was computed. The overall model fit was assessed using an F statistic. The obtained p values were corrected for multiple comparisons using a cortex-based Bonferroni adjustment, i.e., the number of comparisons considered was reduced by limiting the analysis to gray matter voxels (Formisano et al., 2002).

The cortical layout of tonotopic responses was investigated using best-frequency maps. For each voxel with a significant ( $p < 10^{-3}$ , corrected) response to tones, best-frequency was estimated as the frequency at which the averaged stimulus-related BOLD response had the highest amplitude. Maps of best-frequency were obtained by color-coding the estimated best-frequency using two colors (blue and red, see Figure 2) or a logarithmic blue-green-yellow-red color scale (see Figures 3A, 4D, and 5). These maps were projected on folded and morphed (inflated and flattened) polygon meshes ( $\sim 150,000$  vertices) representing the subject's cortical sheet. A continuous representation of best-frequency was obtained by cortical smoothing of the projected map using a 2-neighbor vertices spatial filter.

In subject #2, for each voxel indexed by the cortical maps, frequency tuning curves were computed by fitting the normalized BOLD responses with a Gaussian function. Post hoc estimates of best-frequency and selectivity were obtained, respectively, as the frequency corresponding to the maximum of the Gaussian fit and as the ratio between best-frequency and full-width at half maximum (FWHM) of the Gaussian fit.

Tonotopic field sign maps (Figure 4) were obtained from smoothed versions of a best-frequency map as follows. First, a frequency gradient map was obtained by computing locally the direction of increasing frequency at each vertex of a flattened cortical mesh. Second, a tonotopic axis was defined in correspondence with a line connecting the two high-frequency peaks in the caudo-medial and rostro-lateral portions of activated PAC (see white arrow in the insert in Figure 4A). Finally, gradient directions obtained at each vertex were colored using a binary code: a vertex was color-coded in blue if the associated local direction was included within a  $\pm 90^\circ$  interval centered around the tonotopic axis (see color wheel in the insert in Figure 4A); conversely, a vertex was color-coded in green if the associated local direction corresponded to a mirror representation of the same interval. Note that, whereas two stimulus parameters (polar angle and eccentricity) can be used for an objective definition of a field sign in the retinotopic mapping of the visual cortex (Sereno et al., 1995), in our tonotopic mapping only one stimulus parameter is available (stimulus frequency). In our method the definition of a

tonotopic axis is thus required in order to reduce the sign-mapping problem to one dimension. Our choice for this axis is appropriate for the auditory fields that are activated with high reproducibility in our subjects (see highlighted region in Figure 4). Tonotopic mapping of fields outside this region requires the choice of a different axis.

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